Please replace paragraph number [9164] with the following rewritten paragraph:

[0001] [0164] Lyophilized particles were prepared from tris buffer solutions (5 or 50 mM: pH 7.6) containing hGH (5 mg/mL) using a Durastop μP Lyophilizer in accordance with the following freezing and drying cycles:

Freezing cycle	Ramp down at <u>2.5-2.5° CC/min</u> to -30° C to and hold for 30 min
	Ramp down at 2.5 C 2.5° C/min to -30° C and hold for 30 min
Drying cycle	Ramp up at-0.5 C 0.5° C/min to 10° C and hold for 960 min
	Ramp up at 0.5 C 0.5° C/min to 20° C and hold for 480 min
	Ramp up at 0.5 C <u>0.5° C</u> /min to 25° C and hold for 300 min
	Ramp up at 0.5 C 0.5 C/min to 30 C and hold for 300 min
	Ramp up at 0.5 C 0.5 C/min to 5 C and hold for 5000-5,000 min

Please replace paragraph number [0165] with the following rewritten paragraph:

Example 3

HGHhGH-Stearic Acid Particle Preparation

[0165] Human growth hormone (hGH) particles were prepared as follows: Lyophilized hGH (3.22 grams, Pharmacia-Upjohn, Stockholm, Sweden) and stearic acid (3.22 grams, 95% pure, Sigma-Aldrich Corporation, St. Louis, MO) were blended and ground. The ground material was compressed in a 13 mm round die, with a force of 10,000 pounds for 5 minutes. Compressed tablets were ground and sieved through a 70 mesh screen followed by a 400 mesh screen to obtain particles having a size range between 38 - 212 microns.

Please replace paragraph number [8166] with the following rewritten paragraph:

Example 4

Bupivacaine base Preparation

[0166] Bupivacaine hydrochloride (Sigma-Aldrich Corporation, St. Louis, MO) was dissolved in <u>de-de</u>ionized (DI) water at a concentration of 40 mg/ml (saturation). A calculated amount of sodium hydroxide (in the form of 1 N solution) was added to the solution and the pH of the final mixtures was adjusted to 10 to precipitate the Bupivacaine base. The precipitated product was filtered, and further washed with DI water-for-at at least three times. The precipitated product was dried at ca. 40° C in vacuum for 24-h hours.

Please replace paragraph number [9167] with the following rewritten paragraph:

Example 5

Bupivacaine Particle Preparation

[0167] Bupivacaine drug particles (both base and hydrochloride salt) were prepared as follows. Bupivacaine hydrochloride (Sigma-Aldrich Corporation, St. Louis, MO) or bupivacaine base prepared according to Example 4 were grounded and then sieved to a fixed range using 3" stainless steel sieves. Typical ranges include 25μm to 38μm, 38μm to 63μm, and 63μm to 125μm.

Please replace paragraph number [9169] with the following rewritten paragraph:

Example 7

Preparation of Leuprolide Acetate Particles

[0169] Leuprolide acetate (Mallinckrodt Inc., St. Louis, MI MO) was ground and sieved between 63-125 µm 63-125µm sieves (for nominal particle size of 90 µm 90µm). An GILSON digital Sieve Shaker may be employed to speed the sieving (Gilson Company Inc., Worthington, OH).

[600163] on p.61 of the spec. (b)

Please replace paragraph number [9170] with the following rewritten paragraph:

Example 8

Preparation of Leuprolide Acetate-Stearic Acid Particles

[0170] Stearic acid (95% pure, Sigma-Aldrich Corporation, St. Louis, MO) was passed through a 120-mesh screen (125 μm125μm). Equal amounts of milled leuprolide acetate (463 μm<63μm, prepared as described in Example 2 above) and sieved stearic acid were transferred to the Waring blender and blended for 30 seconds. The blended materials were compressed in a 13 mm round die-using using a compression force of-5000 5,000 lbs and hold time of 5 min. Compressed pellets were ground and sieved through a 120-mesh (125 μm125μm) sieve and retained on a 230 mesh (63 μm63μm) sieve.

Please replace paragraph number [9171] with the following rewritten paragraph:

Example 9

Preparation of Buprenorphine Particles

[0171] Buprenorphine hydrochloride (100 grams, Sigma-Aldrich Corporation, St. Louis, MO) was ground and sieved through pre-preselected sieves such as 25, 38, 62 or 125 micron sieves depending on the desirable particle sizes to obtain the corresponding. Buprenorphine particles.

Please replace paragraph number [9172] with the following rewritten paragraph:

Example 10

Preparation of Buprenorphine-Stearic Acid Particles

Example 4) above above) and stearic acid (prepared as described in Example 3) were blended and ground. The ground material was compressed in a 13 mm round die, with a force of 5,000 pounds for 5 minutes. Compressed tablets were ground and sieved through a 120 mesh screen followed by a 230 mesh screen to obtain particles having a size range between 63-125 microns.

Please replace paragraph number [0174]-with the following rewritten paragraph:

[0174]

Table 4

Formulation	PLGA RG502 ^{4a}	LMW PLGA	Benzyl
	(wt%)	(wt%)	Benzoate
			(wt%)
17 ^{4c}	45	0 ^{4b}	45
18 ^{4c}	0	45 ^{4b}	45
19 ^{4d}	45	0^{4b}	45
20 ^{4d}	0	45 ⁴⁶	45
21 ^{4f}	45	0 ^{4e}	° 45
22 ^{4f}	0	45 ^{4e}	45
23 ^{4f}	0	63 ^{4e}	27

4a = PLGA RG 502, MW = 16,000.

4b = Low Molecular Weight (LMW, MW = 8000 8,000) PLGA with an ester end group.

4c = 10% bupivacaine hydrochloride loading.

4d = 10% bupivacaine base loading.

4e = Low Molecular Weight (LMW, MW - 7,000) PLGA with an ester end group

4f = 5% hGH loading.

Table 5

Formulation	LMW	LMW	Benzyl.	Benzyl
	PLGA ^{5g}	PLGAc ^{5h}	Benzoate	Alcohol
	(wt%)	(wt%)	(wt%)	(wt%)
2451	58.5	0	31.5	0
25 ⁵ⁱ	58.5	0	0	31.5
26 ⁵ⁱ	67.5	0	0	22.5
27 ⁵ⁱ	0	67.5		22.5
28 ^{5j}	0	60		20

5g = Low Molecular Weight (LMW, MW = 8,000) PLGA with an ester end group.

5h = Low Molecular Weight (LMW, MW = 10,000) PLGA with a carboxyl end group.

5i = 10% bupivacaine hydrochloride loading.

5j = 10% bupivacaine hydrochloride and 10% SA loading.

Table 12

Formulation	P(DL)LA R202 (wt%)	BB (wt%)	BA (wt%)
58 ^{12a,b}	50.6	41.4	-
59 ^{12a,b}	50.6	•	41.4
60 ^{12b,c}	55.0	45.0	-
61 ^{12b,c}	55.0	-	45.0

12a = 8 wt% 8 wt.% leuprolide acetate loaded;

12b = 100 mg depot injection per rat;

12c = Placebos without leuprolide acetate.

Please replace paragraph number [9175] with the following rewritten paragraph:

Example 12

Rheological Properties-Of of Depot Formulations

[0175] In general, viscosity of the depot vehicle formulations was tested using a Bohlin CVO 120 rheometer (Bohlin Instruments, Cranbury, NJ). All testing-were was performed at 24° C using 20 mm parallel plates. The viscosity of various gel formulations or leuprolide acetate depot formulations of the invention, as tabulated in Tables 6-12, was tested as described above. As illustrated in Figures 1, 2 and 3, the depot formulations (Formulations # 42-48, 51 and 52) have different rheological properties. Thus, the depot formulations with with a wide range of viscosities can be achieved by the combination of different polymers (PLGA type, molecular weight etc.), solvent or co-solvent; and different polymer/solvent ratios according to the present invention.

Please replace paragraph number [9176] with the following rewritten paragraph:

Example 13

Injection force of leuprolide acetate depot formulations

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Please replace paragraph number [9177] with the following rewritten paragraph:

[0177] The injection force of various gel formulations or leuprolide acetate depot formulations of the invention, as tabulated in Tables 6-12, was tested as described above. As illustrated in Figures 4 and 5, the depot formulations (Formulations 42-45 and 48-50) have different injection forces. Thus, depot formulations with different injection forces can be tailored by the combination of different polymers (PLGA type, molecular weight etc.), solvent or co-solvent, different or different polymer/solvent ratios according to the present invention.

Please replace paragraph number [0178] with the following rewritten paragraph:

Example 14

In Vitro Release Rate Profiles of Depot Gel Formulations

[0178] A representative number of implantable gels were prepared in accordance with the foregoing procedures and tested for *in vitro* release of beneficial agent as a function of time. In general, the *in vitro* release of bioactive agent from the depot formulation of the present invention was performed as follows. The depot gel formulation (80-120 mg) was loaded into a tea bag and placed in a 20 mL scintillation vial and the release medium (5 mL, phosphate buffer saline (PBS) + 0.1% Tween 20, pH 7.4) was added to the vial. The vial was incubated in a 37° C water bath with gentle agitation. The medium was replaced daily for the first 5 days, then twice a week thereafter-till_until the end-of_of the release duration. The amount of bioactive agent released from the depot was measured by various methods dependent-the on the nature of the bioactive agent: size exclusion chromatography high pressure liquid chromatography (SEC HPLC) is generally used for protein, while reverse phase high pressure liquid chromatography (rpHPLC) or ultraviolet (UV) techniques are generally used for small molecular compounds.

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[00072] Starting on p.67 of the spec. W)
Please replace paragraph number [0180] with the following rewritten paragraph:

[0180] In general, in vivo studies in rats were performed following an open protocol to determine plasma levels of the beneficial agent (e.g., hGH, bupivicaine, leuprolide, buprenorphine) upon systemic administration of the beneficial agent via the implant systems of this invention. Depot gel formulations containing the beneficial agent (prepared as described in the Examples above) were loaded into 0.25 cc-or a or 0.5 cc disposable syringes (e.g.e.g., Hamilton Gastight syringes) or catheters. Disposable needles (16 gauge or 18 gauge) were attached to the syringes and were heated to 37° C using a circulator bath. The depot gel formulations (as tabulated in Tables 1-12) were injected into rats and blood was drawn at specified time intervals. All plasma samples were stored at 4° C prior to analysis. Samples were analyzed for the beneficial agent using any one of the following methods: radio immuno assay (RIA) or validated LC/MS/MS method (Ricerca, LLC, Painesville, Ohio).

Please replace paragraph number [0181] with the following rewritten paragraph:

Example 16

hGH In Vivo Studies

[0181] A representative number of implantable gels as tabulated in Tables 4-6 were tested for in rats to determine vivo in vivo release rate profiles as described in Example 15 above. In particular, depot gel hGH compositions were injected from customized 0.5 cc disposable syringes having disposable 16 gauge needles, into rats and blood was drawn at specified time intervals. The release rate profile of hGH from various depot gel formulations was determined by measuring the blood serum or plasma concentrations of hGH as a function of time, as illustrated in Figure Figures 6-6A-D (formulations 21, 22, 29-31, and 33-40). Samples were analyzed for intact hGH content using a radio immuno assay (RIA).

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Please replace paragraph number [0182] with the following rewritten paragraph:

Example 17

Bupivacaine In Vivo Studies

[0182] A representative number of implantable gels as tabulated in Table 4 were tested for in rats to determine vivo in vivo release rate profiles as described in Example 15 above. In particular, depot gel bupivacaine compositions were injected from customized 0.5 cc disposable syringes having disposable 18 gauge needles, into rats and blood was drawn at specified time intervals (1 hour, 4 hours and on days 1, 2, 5, 7, 9 and 14, 21 and 28) and analyzed for bupivacaine using LC/MS. Figures 7, 8 and 9 illustrate representative in vivo release profiles of bupivacaine hydrochloride (formulations 17 and 18) and bupivacaine base (formulations 19 and 20) obtained in rats from various depot formulation, formulations, including those of the present invention. The in vivo release profile of the depot formulations with low molecular weight PLGA (formulations 18 and 20 in Figures 7, 8 and 9) exhibited a shorter release duration of approximately 7 days, as compared to the control formulations (with higher molecular weight PLGA, formulations 17 and 19).

Please replace paragraph number [0183] with the following rewritten paragraph:

Example 18

Bupivacaine In Vivo Studies

tested for in rats to determine-vivo in vivo release rate profiles as described in Example 17 above. Figures 10 and 11 illustrate representative in vivo release profiles of bupivacaine obtained in rats from various depot-formulation, formulations, including those of the present invention. As illustrated in the figures, when the same amount of bupivacaine was administrated, the duration of the in vivo sustained release of bupivicaine from the formulation is directly proportional to the percent loading of bupivacaine within the depot gel composition. In particular, at 10% bupivicaine HCl loading, the amount of bupivicaine released increased with time after an initial decline during the first two weeks. Although not wanting to be limited to a particular theory, the

results indicate that the early stage diffusion mechanism may be the primary mechanism contributing to the release of the beneficial agent, while at later stages, polymer degradation might significantly contribute to the release.

Table 13

Formulation	PLGA RG502 (wt%)	Benzyl Benzoate (wt%)	Bupivacaine (wt%)
62	35	35	30 ^{13a}
63	45	45	10 ^{13a}
64	35	35	30 ^{13b}
65	45	45	10 ^{13b}

a = particle size of bupivacaine is ca. $\frac{35 \mu m}{35 \mu m}$;

b = particle size of bupivacaine is ca. $\frac{90 \mu m}{90 \mu m}$.

Please replace paragraph number [9184] with the following rewritten paragraph:

Example 19

In Vivo Studies on Bupivacaine Depot Composition With Different PLGA

Molecular Weight Distributions

[0184] A representative number of implantable gels as tabulated in Table 2 were tested for in rats to determine-vivo in vivo release rate profiles as described in Example 15 above. In particular, depot gel bupivacaine compositions were injected from customized 0.5 cc disposable syringes having disposable 18-18-gauge needles, into rats and blood was drawn at specified time intervals (1 hour, 4 hours and on days 1, 2, 5, 7, 9 and 14, 21 and 28) and analyzed for bupivacaine using LC/MS. Figure 12 illustrates the representative in vivo release profiles of bupivacaine obtained in rats from the formulations 11 and 12 (the bupivacaine depots were formulated with the PLGAs with two different molecular weight distributions in benzyl benzoate (single-modal containing MMW PLGA RG502, and bi-modal mixture of HMW PLGA RG503 with LMW PLGA, Table 2 formulations 11 and 12).

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[000177] on p.70 of the Spec. When Please replace paragraph number [9185] with the following rewritten paragraph:

Example 20

In Vivo Release Rate Profiles of

Various Leuprolide Acetate Depot Formulations

[0185] A representative number of implantable gels as tabulated in Tables 7-9 were tested for in rats to determine vivo in vivo release rate profiles as described in Example 15 above. In particular, release the release rate profile of leuprolide was determined by measuring the blood serum or plasma concentrations of leuprolide as a function of time, as illustrated in Figures 13-16.

Please replace paragraph number (0186) with the following rewritten paragraph:

In particular, Figure 13 illustrates representative in vivo release profiles of leuprolide acetate obtained in rats from depot formulations according to the present invention containing PLGA (L/G: 75/25) in either benzyl benzoate (BB) (formulation 42) or benzyl alcohol (BA) (formulation 47), as compared to a commercial 3-month leuprolide acetate depot, Lupron depot® (formulation 53). Figure 14 illustrates representative in vivo release profiles of leuprolide acetate obtained in rats from depot formulations according to the present invention containing PLGA (L/G: 75/25) in benzyl benzoate, mixture a mixture of benzyl benzoate and benzyl alcohol, or benzyl benzoate with ethanol as a thixotropic agent (formulations 42, 43 and 45, respectively). Figure 15 illustrates representative in vivo release profiles of leuprolide acetate obtained in rats from depot formulations according to the present invention containing PLGA (L/G: 75/25) in benzyl benzoate with the drug particles formulated either with or without stearic acid (formulations 42 & 49). Figure 16 illustrates representative in vivo release profiles of leuprolide acetate obtained in rats from depot formulations according to the present invention containing poly(caprolactone-co-lactic acid) (PCL-co-LA) (CL/L: 25/75) in benzyl benzoate (formulation 46) as compared to a commercial 3-month leuprolide acetate depot, Lupron depot[®] (formulation 53 - from TAP (The front chamber of Lupron depot[®]-3-month 3-month 11.25 mg prefilled dual-chamber syringe containing leuprolide acetate (11.25 mg),

polylactic acid (99.3 mg) and D-mannitol (19.45 mg). The second chamber of diluent contains carboxymethylcellulose sodium (7.5 mg), D-mannitol (75.0 mg), polysorbate 80 (1.5 mg), water for injection, USP and glacial acetic acid, USP to control pH.)).

Please replace paragraph number [0188] with the following rewritten paragraph:

Example 21

In Vivo Release Rate Profiles of

Various Leuprolide Acetate Depot Formulations

[0188] A representative number of implantable gels as tabulated in Table 10 were tested for in rats to determine vivo in vivo release rate profiles as described in Example 15 above. In particular, release the release rate profile of leuprolide was determined by measuring the blood serum or plasma concentrations of leuprolide as a function of time, as illustrated in Figure 17.

Please replace paragraph number [0189] with the following rewritten paragraph:

[0189] In particular, Figure 17 illustrates representative *in vivo* release profiles of leuprolide acetate obtained in rats from depot formulations according to the present invention containing P(DL)LA in benzyl benzoate (BB) with different polymer/solvent ratios (formulation formulations 51 and 52), as compared to the 3 month durational depot formulation (formulation 42) and a commercial 3-month leuprolide acetate depot, Lupron depot® (formulation 53).

Please replace paragraph number [0190] with the following rewritten paragraph:

[0190] As illustrated in Figure 17, sustained release of leuprolide acetate from the depots formulation depot formulations of the invention can be achieved for a duration greater than or equal to 6 months by using the biodegradable polymer with longer degradation duration. The release profiles of the active agent from the depots can be varied by varying the type of polymer and solvent, and by varying the polymer/solvent ratios.

Please replace paragraph number [9191] with the following rewritten paragraph:

Example 22

InVivo Release Rate Profiles of Various-BuprEnorphine Buprenorphine Depot

Formulations

[0191] A representative number of implantable buprenorphine depot gel formulations of the present invention are tested for in rats to determine-vivo in vivo release rate profiles as described in Example 15 above. In particular, release the release rate profile of buprenorphine is determined by measuring the blood serum or plasma concentrations of leuprolide as a function of time. The release profiles of the active agent from the depots can be varied by varying the type of polymer and solvent, and by varying the polymer/solvent ratios.

Please replace paragraph number [0192] with the following rewritten paragraph:

Example 23

In Vivo Testosterone Suppression by Depot Gel Leuprolide Formulations [0192] In general, in vivo studies in rats were performed following an open protocol to determine plasma levels of leuprolide upon systemic administration of leuprolide via the implant systems of this invention. Depot gel leuprolide formulations (prepared as described in Examples above) were loaded into 0.25 cc Hamilton Gastight syringes. Disposable 18-18-gauge needles were attached to the syringes and were heated to 37° C using a circulator bath. Depot gel leuprolide acetate formulations were injected into rats and blood was drawn at specified time intervals. All plasma samples were stored at 4° C prior to analysis. Samples were analyzed for leuprolide as described in Example 15 above, and for testosterone using a commercially available RIA kit (DSL-4000) (Ricerca, LLC, Painesville, Ohio).

[000185] on p.73 of the spec. (1) Please replace paragraph number [0193] with the following rewritten paragraph:

Example 24

InVivo In Vivo Release Rate Profiles and Efficacy of Various Leuprolide Acetate Depot Formulations

[0193] A representative number of implantable gels as tabulated in Table 11 were tested for in rats to determine-vivo in vivo release rate profiles and efficacy as measured by testosterone suppression as described in Example 23 above. In particular, release the release rate profile of leuprolide and efficacy, i.e. i.e., testosterone suppression, were determined by measuring the blood serum or plasma concentrations of leuprolide and testosterone as a function of time, as illustrated in Figure 18.

Please replace paragraph number [9195] with the following rewritten paragraph:

Example 25

InVivo In Vivo Release Rate Profiles and Efficacy of Various Leuprolide Acetate Depot Formulations

[0195] A representative number of implantable gels as tabulated in Table 12 were tested for in rats to determine vivo in vivo release rate profiles and efficacy as measured by testosterone suppression as described in Example 23 above. In particular, release the release rate profile of leuprolide and efficacy, i.e. i.e., testosterone suppression, were determined by measuring the blood serum or plasma concentrations of leuprolide and testosterone as a function of time, as illustrated in Figure 20.

Please replace paragraph number [9196] with the following rewritten paragraph:

[0196] In particular, Figure 20 illustrates representative in vivo sustained release profiles of leuprolide acetate obtained in rats from depot formulations according to the present invention containing P(DL)LA in either benzyl benzoate (BB) or benzyl alcohol (BA) for 6 months (formulations 58 and 59). Figure 21 illustrates the testosterone profiles of the leuprolide acetate depot formulations (formulations 58 and 59) as compared to the placebos without